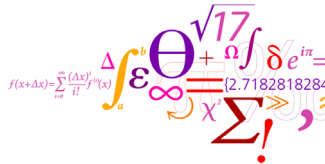


# Medical Diagnostic Ultrasound: *Imaging and interaction with tissue*

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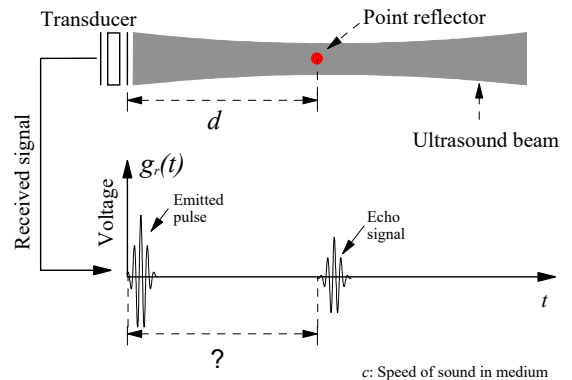
## Content

- Imaging by the pulse-echo technique
  - A, M and B mode
  - Spatial resolution size
- Interaction with tissue
  - Plane waves
  - Transmission and reflection
  - Scattering
  - Attenuation
- Special issues
  - Speckle
  - Geometrical effects
  - Other effects (shadows)

## Pulse-echo imaging

- Images consist of scan lines
- A scan line appears as a rectangular bar, or region, with a gray tone level proportional to the log of the envelope of the echo signal from the direction it represents

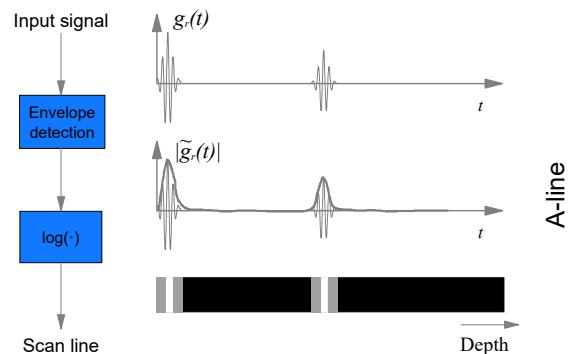
## Basic principle in imaging (pulse-echo mode)



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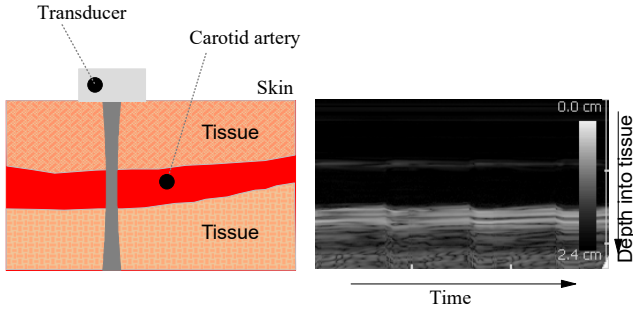
## Creating one scan line



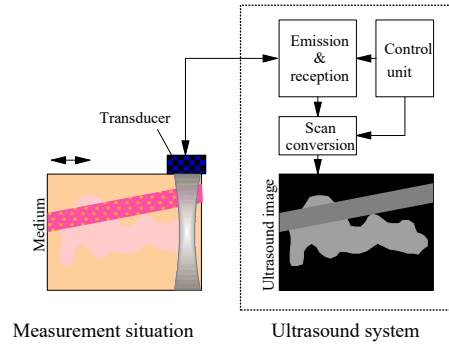
# M-mode image of vessel wall

Measurement situation

M-mode image



# Building the image with scan lines



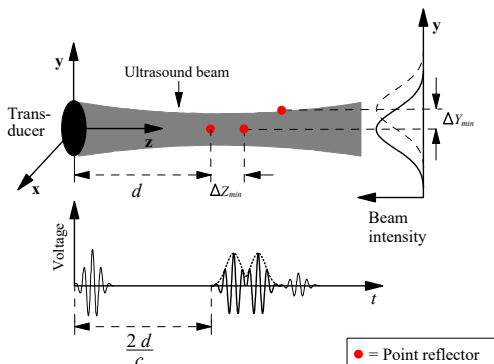
# Animation of B-mode imaging

Please see Webbook

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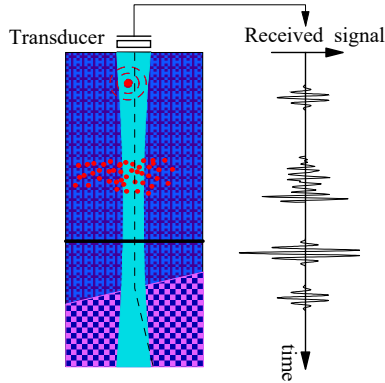
# Spatial resolution size



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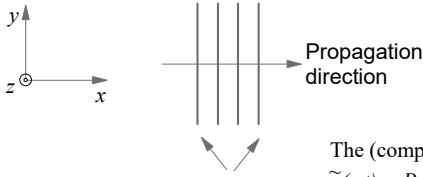
# Ultrasound's interaction with tissue



# Content

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# Plane waves



At any given plane perpendicular to this picture, all acoustic parameters are constant.

The (complex) pressure is:  

$$\tilde{p}(x,t) = P_0 \exp(-j(2\pi f_0 t - 2\pi x/\lambda))$$

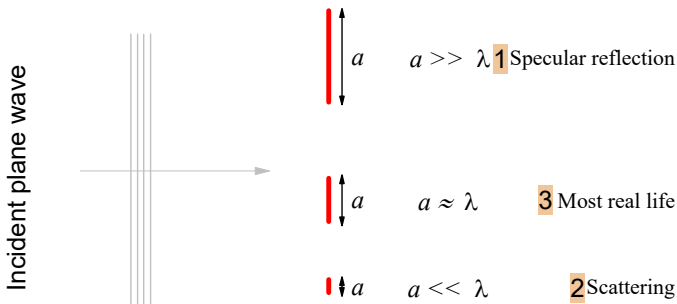
where:  
 $\lambda = c/f_0$   
 and  
 $f_0 =$  (CW) frequency of the wave  
 $c =$  the speed of sound

# (Monochromatic) Plane waves

- Are mathematically easy to describe
- Only exist in theory
- Have one frequency and one direction
- "Behaves" as rays in the propagation direction
- Analogies to signal analysis:
  - A plane wave correspond to an infinite tone signal

# Organization

Size matters!



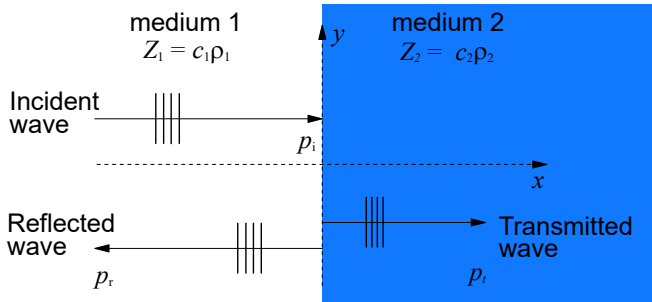
! = Interface generating an echo.  $\lambda =$  wavelength

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## Transmission and reflection:

### Normal incidence

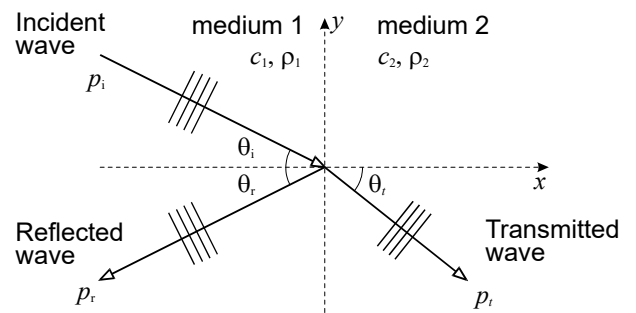


$Z_1$  = specific acoustic impedance.

$r_p = (Z_2 - Z_1) / (Z_1 + Z_2)$  = amplitude reflection coef.  $-1 \leq r_p \leq 1$

## Transmission and reflection:

### Oblique incidence



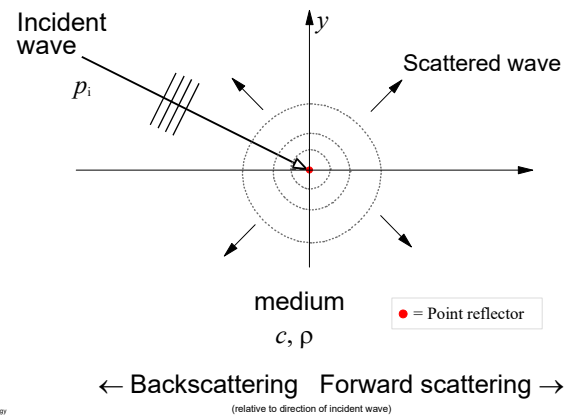
$\theta_i$  and  $\theta_r$  are governed by Snell's law (see notes)

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## Scattering:



## Summarizing



Echoes in biological tissue are generated by a situation *in-between*:

- **Specular reflection from infinitely large interfaces** between materials of different acoustic impedance
- **Scattering from infinitely small point targets** with acoustic impedance different from the surroundings

## Examples



Specular reflection from large interfaces:

- 
- 

Scattering from small point targets:

- 
- 

Echo from "structures":

- 
-

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## Attenuation (Kinsler & Frey) :



- 1) Absorption (conversion of acoustic energy to heat):
  - Viscous losses
  - Heat conduction losses and
  - Molecular exchanges of energy
- 2) Losses due to scattering and reflection

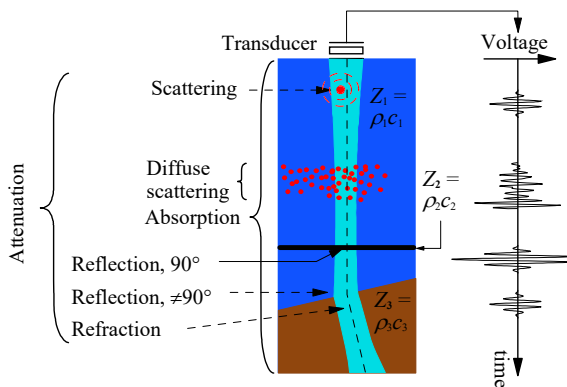
The intensity of the forward propagating wave:

$$I(z) = I(0) \exp(-\alpha z)$$

where  $\alpha$  [ $\text{m}^{-1}$ ] is the *attenuation coefficient* and  $z$  is distance traveled.

For typical tissue, the attenuation is 1 dB/cm/MHz

## Ultrasound's interaction with tissue



## Selected tissue parameters



Medium	Density ( $\text{kgm}^{-3}$ )	Specific acoustic impedance ( $\text{kgm}^{-2}\text{s}^{-1}$ )
Air	1.2	$0.4 \times 10^3$
Fat	$0.92 \times 10^3$	$1.33 \times 10^6$
Water	$1.00 \times 10^3$	$1.53 \times 10^6$
Kidney	$1.04 \times 10^3$	$1.62 \times 10^6$
Liver	$1.06 \times 10^3$	$1.66 \times 10^6$
Blood	$1.06 \times 10^3$	$1.66 \times 10^6$
Muscle	$1.07 \times 10^3$	$1.70 \times 10^6$
Bone	$1.62 \times 10^3$	$4-7.5 \times 10^6$

● = Soft tissues

## $\mu$ -Problem:



What is the amplitude reflection coefficient between blood and muscle (assuming normal incidence)?

## $\mu$ -Solution:



The amplitude reflection coefficient between blood ( $Z_1$ ) and muscle ( $Z_2$ ):

$$r_p = \frac{Z_2 - Z_1}{Z_1 + Z_2}$$

$$= \frac{(1.7 - 1.66)}{(1.66 + 1.7)} = \underline{\hspace{2cm}} \%$$

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## Speckle



Many sub-resolvable scatterers are normally present in the ultrasound beam

⇒ random interference pattern between the echoes of the individual scatterers

⇒ Resulting echo signal might have a highly fluctuating amplitude

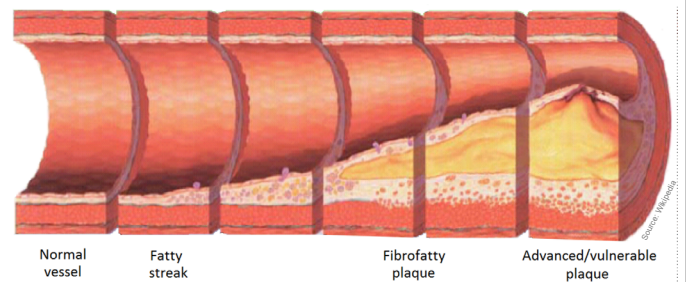
Show pulse\_echo program

## Content

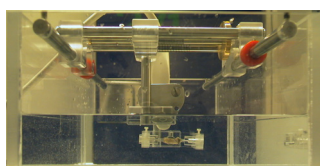
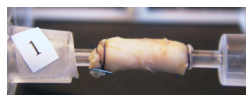


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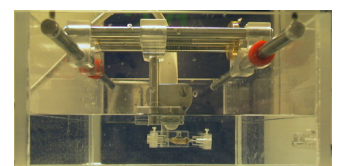
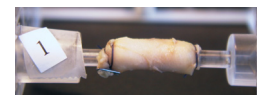
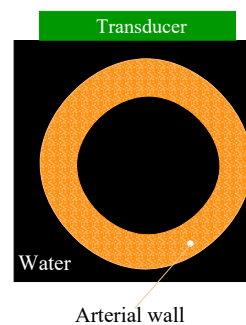
## Atherosclerosis



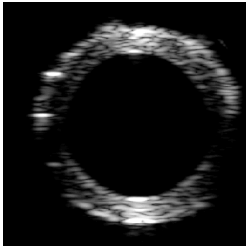
## Principle of measurement situation



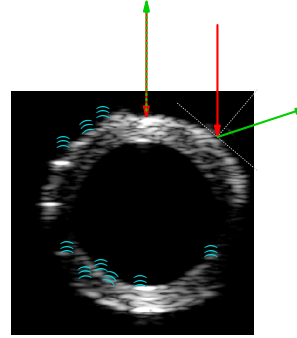
## Principle of measurement situation



## Conventional ultrasound image

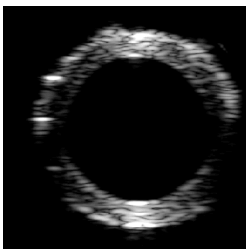


## Conventional ultrasound image



- Specular reflection:**
  - Smooth, curved structures
  - Phase cancellation in transverse surface
- Scattering:**
  - Independent on angle
- Interference:**
  - Provides the speckle pattern

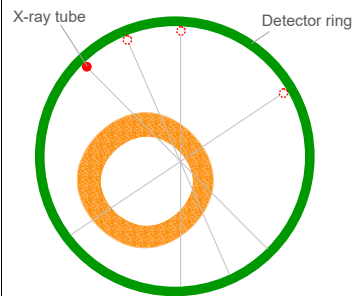
## Conventional ultrasound image



- Known tissue: ☺
- Unknown tissue: ☹
- Atherosclerosis: ☹

## Comparison with CT

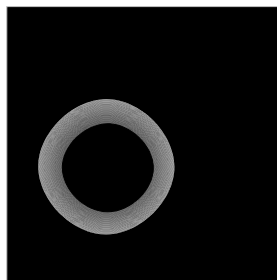
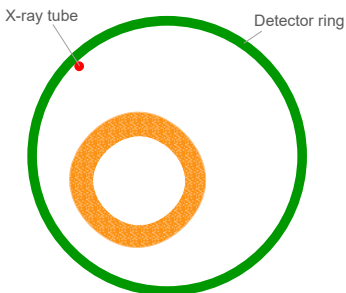
### Recording of CT image



## Comparison with CT

### Recording of CT image

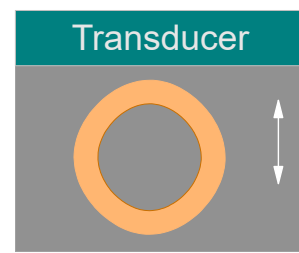
### CT image



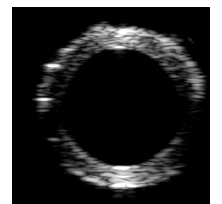
## Conventional B-mode image

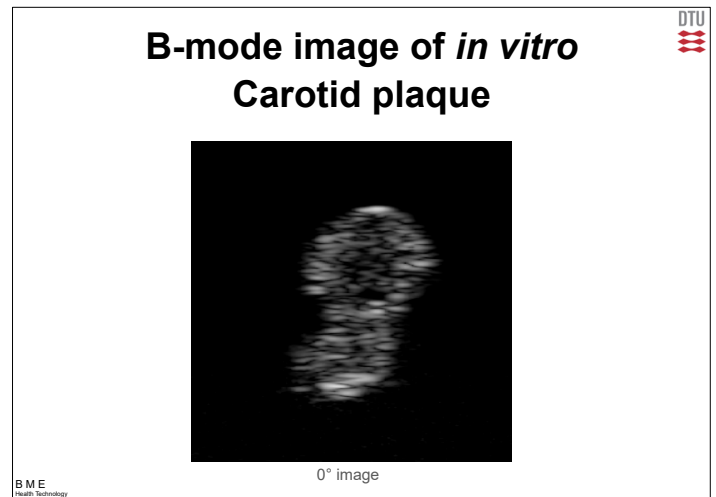
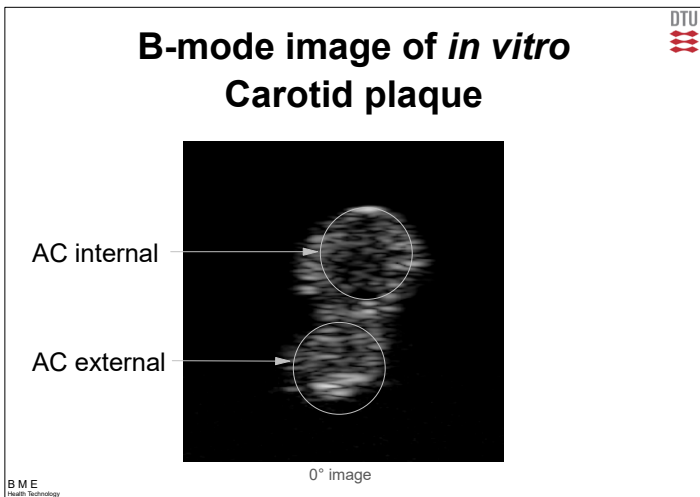
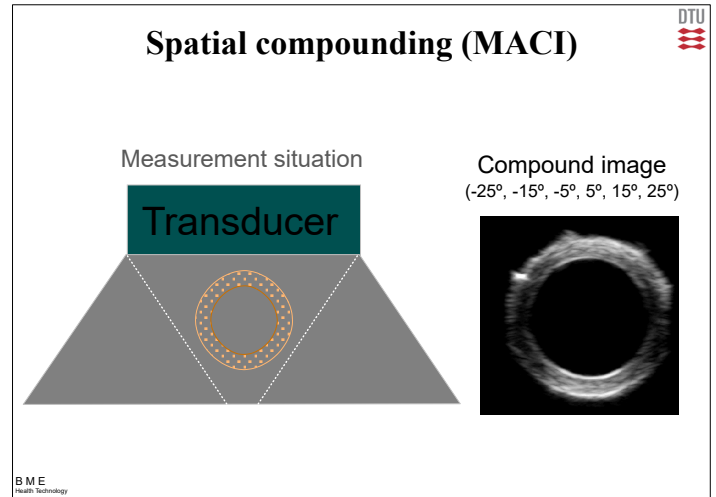
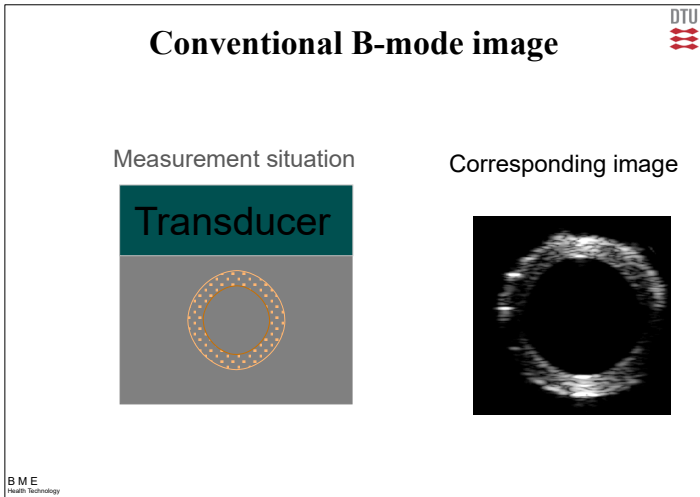
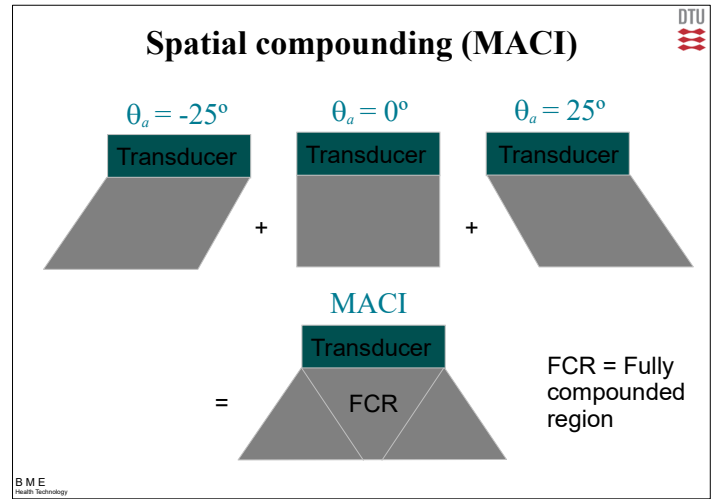
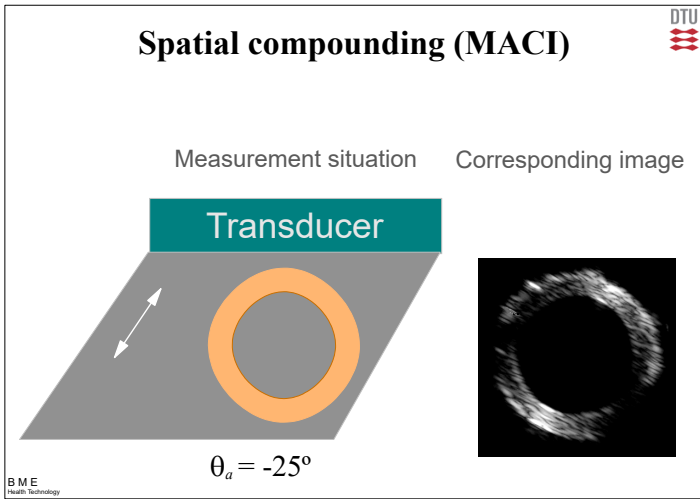
### Measurement situation

### Corresponding image



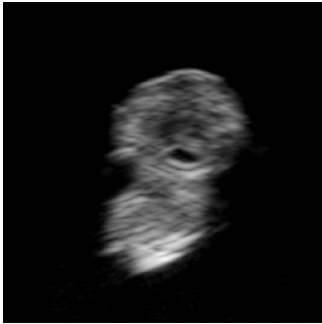
$$\theta_a = 0^\circ$$







# Compound image of *in vitro* Carotid plaque

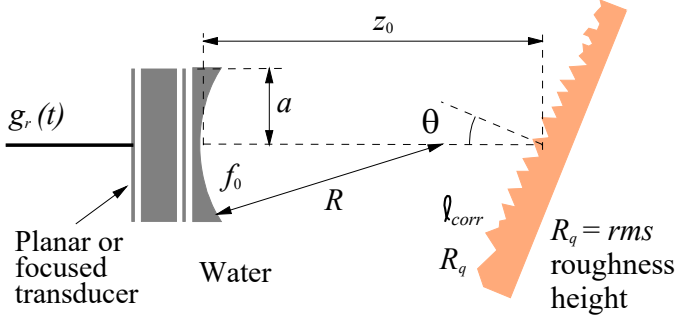


Average of 7 single-angle images

# Angle-dependence

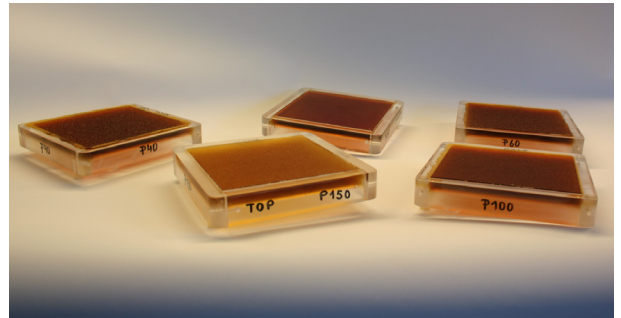
- ▣ Modelling
- ▣ Measurements (rough surfaces)

# Simplified measurement set-up



$$E(\theta, z_0, R_q) = \int |\tilde{g}_r(t, \theta, z_0, R_q)|^2 dt$$

# Rough surfaces



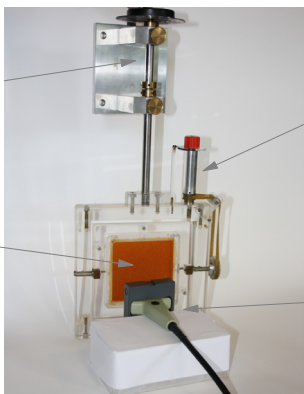
# Dual-angle rotation holder

Axis for azimuth angle

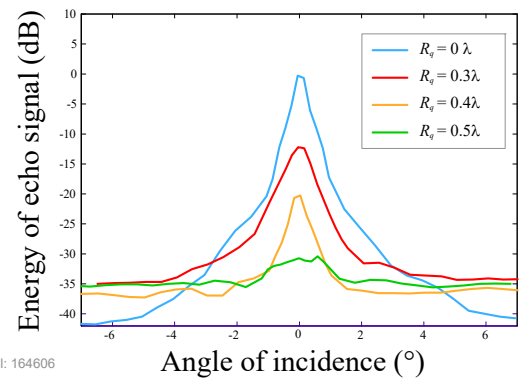
Axis vertical angle

Rough surfaces goes here

Array-transducer



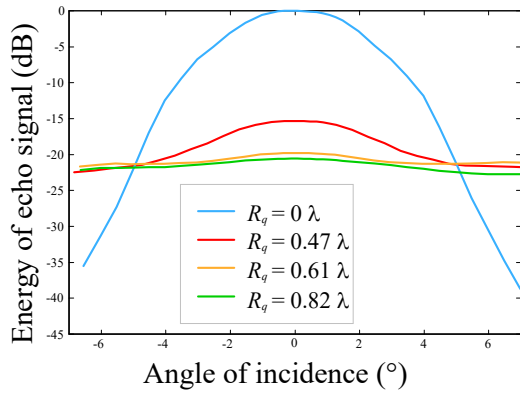
# Energy of received signal, $E(\theta, z_0, R_q)$ (5 MHz planar transducer, $a = 12.7$ mm, $z_0 = 70.4$ mm)



Serial: 164606

## Energy of received signal, $E(\theta, z_0, R_q)$

(7.5 MHz focused transducer,  $a = 6.35$  mm  $R = 58.5$  mm,  $z_0 = 58.5$  mm)

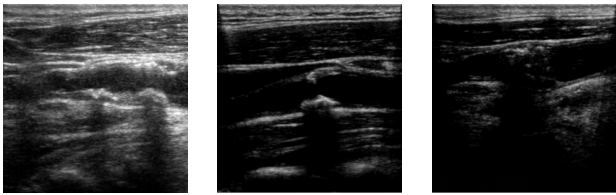


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## Shadows

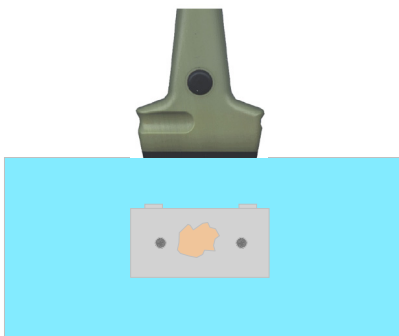


Images of atherosclerotic Carotid plaque causing shadows

## Measurements in this course

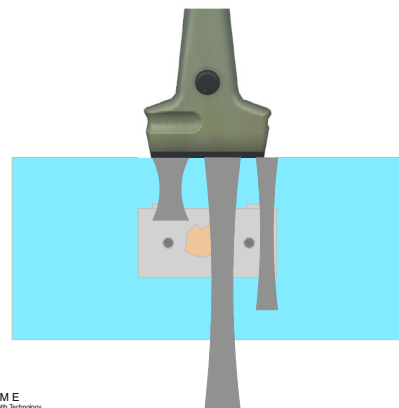


## Measurements in this course



• Before recording:

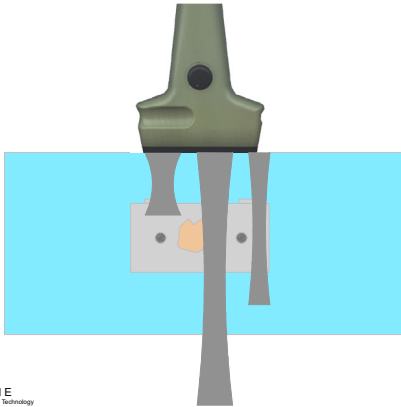
## Measurements in this course



• Before recording:
 

- Depth of image
- Transmit focal point

# Measurements in this course



- Before recording:
  - Depth of image
  - Transmit focal point
- After recording:
  - Note transducer frequency
  - Are pixels quadratic in size?
  - How to find axis?